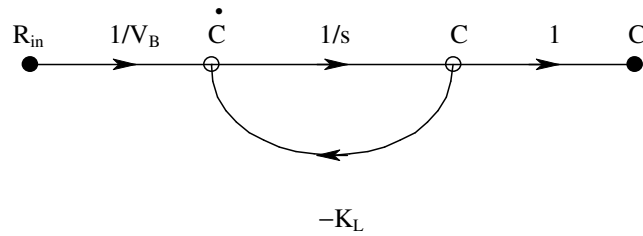


Chapter 2 Home Problem Solutions

2.1 A) SFG for the simple, one-compartment drug infusion system:



$$\frac{C}{R_{in}}(s) = \frac{(1/V_B)}{s + K_L} \quad \text{Transfer function.}$$

B) Let $R_{in}(t) = R_o \delta(t)$, $\therefore R_{in}(s) = R_o$, and by inverse LT tables: $c(t) = (R_o/V_B)e^{-K_L t}$, $t \geq 0$.

C) Let $R_{in}(t) = R_d U(t)$: $\therefore R_{in}(s) = R_d/s$, and by inverse LT tables: $c(t) = (R_d/K_L)(1 - e^{-K_L t})$, $t \geq 0$. The $c_{ss} = R_d/K_L$ as $t \rightarrow \infty$.

2.2 LTI system described by 2nd order ODE:

$$\ddot{y} + 7\dot{y} + 10y = x(t)$$

A) $y[p^2 + 7p + 10] = x(t)$; factoring, we find: $y[(p+2)(p+5)] = x$. Thus $p_1 = -2$, $p_2 = -5$.

B) Use Laplace transforms, find xfer function:

$$\frac{Y}{X}(s) = \frac{1}{(s+2)(s+5)}$$

a b

Let $x(t) = \delta(t)$, so $X(s) = 1$. The inverse Laplace transform table gives us:

$$y(t) = \frac{1}{(5-2)}[e^{-2t} - e^{-5t}]$$

b a

C) Now let there be a step input, $x(t) = 10U(t)$, so $X(s) = 10/s$: The inverse Laplace transform is:

$$y(t) = \frac{10}{(2)(5)} \left[1 + \frac{1}{(2-5)}(5e^{-2t} - 2e^{-5t}) \right] = 1 \left[1 - 1/3(5e^{-2t} - 2e^{-5t}) \right]$$

a b

2.3 A) There are two compartments: V_B liters of blood, V_E liters of extracellular fluid.

The ODEs describing the system are:

$$\begin{aligned} \dot{C}_B V_B &= -K_{LB} C_B - K_{DBE} (C_B - C_E) + R_{in} && \mu\text{g/min.} \\ \dot{C}_E V_E &= +K_{DBE} (C_B - C_E) && \mu\text{g/min.} \end{aligned}$$

These ODEs can be rewritten in terms of concentrations:

$$\begin{aligned} \dot{C}_B &= -C_B(K_{LB} + K_{DBE})/V_B + C_E(K_{DBE}/V_B) + R_{in}/V_B \quad (\mu\text{g/l})/\text{min.} \\ \dot{C}_E &= +C_B(K_{DBE}/V_E) - C_E(K_{DBE}/V_E) \quad (\mu\text{g/l})/\text{min.} \end{aligned}$$

This system and its linear SFG is illustrated on **Page 2B**.

B) Consider the system to be in the DC steady state, so \dot{C}_B & $\dot{C}_E = 0$. Thus we can write:

$$C_B(K_{LB} + K_{DBE})/V_B - C_E(K_{DBE}/V_B) = R_{in}/V_B$$

$$C_B(K_{DBE}/V_F) - C_F(K_{DBE}/V_F) = 0$$

The second equation above tells us that $C_B = C_E$ in the SS. The first equation can easily be solved for C_B in the

SS:

$$C_{BSS} = C_{ESS} = R_d / K_{LB}. \quad (R_d \text{ is the IV drip rate in } \mu\text{g}/\text{min}.)$$

C) A bolus injection gives the PK system's impulse response. First we use Mason's rule to obtain the system's transfer function, $\frac{C_B}{R_{in}}(s)$, and note that $R_{in}(t) = R_o\delta(t)$, so $R_{in}(s) = R_o$. The C_B transfer function is, after some algebra:

$$\frac{C_B}{R_{in}} = \frac{(1/V_B)(1/s)[1 - (-K_{DBE}/(V_E s))]}{1 - \{-(K_{LB} + K_{DBE})/(V_B s) - K_{DBE}/(V_E s) + K_{DBE}^2/(V_E V_B s^2)\} + \{-(K_{LB} + K_{DBE})/(V_B s) \times -K_{DBE}/(V_E s)\}}$$

$$C_B(s) = \frac{(R_0/V_B) (s + K_{DBE}/V_E)}{s^2 + s [(K_{LB} + K_{DBE})/V_B + K_{DBE}/V_E] + [(K_{LB} + K_{DBE})/V_B \times K_{DBE}/V_E - K_{DBE}^2/(V_E V_B)]}$$

Subbing numbers:

$$C_B(s) = \frac{R_o 0.33333 (s + 0.06667)}{s^2 + s[0.73333] + 0.02222}, \text{ Factoring the denominator, } C_B(s) = \frac{R_o 0.33333 (s + 0.06667)}{(s + 1.4325)(s + 0.03412)}$$

The inverse Laplace transform yields: $C_B(t) = R_o \frac{0.33333}{1.39838} \{ 0.03255 e^{-0.03412t} - (-1.3658)e^{-1.4325t} \}$

2.4 An underdamped, quadratic LPF is described by the second-order ODE:

$$\ddot{y} + (2\xi\omega_n)\dot{y} + \omega_n^2 y = x(t)$$

A) Find the root locations in the complex s-plane: Laplace Xform the ODE:

$Y(s)[s^2 + (2\xi\omega_n)s + \omega_n^2] = X(s)$: The complex-conjugate roots (poles) of the denominator are thus:

$$s_1, s_2 = -\xi\omega_n \pm \frac{1}{2}\sqrt{(4(\xi\omega_n)^2 - 4\omega_n^2)} < 0 = -\xi\omega_n \pm j\omega_n\sqrt{(1 - \xi^2)} = -0.5 \pm j 0.8660 \text{ (poles lie in the left-half}$$

s-plane). The filter's Xfer function is thus:

$$\frac{Y(s)}{X(s)} = \frac{1}{[s^2 + (2\xi\omega_n)s + \omega_n^2]} = \frac{1}{s^2 + 1s + 1}$$

B) The filter's *unit step response* can be found by inverse Laplace Xform tables:

$$Y(s) = \frac{1}{s} \frac{1}{[s^2 + (2\xi\omega_n)s + \omega_n^2]}: y(t) = \frac{1}{\omega_n^2} \left\{ 1 - \frac{e^{-\xi\omega_n t}}{\sqrt{1 - \xi^2}} \sin[\omega_n \sqrt{1 - \xi^2} t + \phi] \right\}, \text{ where } \phi = \tan^{-1} \left[\frac{\sqrt{1 - \xi^2}}{\xi} \right]$$

C) The filter's unit impulse is:

$$Y(s) = \frac{1}{[s^2 + 1s + 1]}. \text{ Inverse transforming: } y(t) = (1/\omega_n) \frac{e^{-\xi\omega_n t}}{\sqrt{1 - \xi^2}} \sin[\omega_n \sqrt{1 - \xi^2} t]$$

$\omega_n = 1 \text{ r/s}$, $\xi = 0.5$, so $y(t) = 1.1547 e^{-0.5t} \sin[0.866 t]$, so $y(t) = 1.1547 e^{-0.5t} \sin[0.866 t]$

2.5 Alternative ODE form for an underdamped, quadratic LPF:

$$\ddot{y} + 2a\dot{y} + (b^2 + a^2)y = x(t)$$

Note $\omega_n^2 \equiv (b^2 + a^2)$, & $(2\xi\omega_n) \equiv 2a$, so $a = \omega_n\xi$, and $\omega_n^2 = b^2 + \omega_n^2\xi^2 \rightarrow$ thus $b^2 = \omega_n^2(1 - \xi^2) \rightarrow b = \omega_n\sqrt{1 - \xi^2}$

A) The filter's Xfer function is:

$$\frac{Y(s)}{X(s)} = \frac{1}{s^2 + 2as + (b^2 + a^2)} \quad 2a = 1, (b^2 + a^2) = 0.7500 + 0.25 = 1, \text{ thus the denom. is: } s^2 + s + 1$$

The denominator roots (poles) are at: $s_1, s_2 = -0.5 \pm \frac{1}{2} \sqrt{1-4} = -0.5 \pm j 0.8660$.

B) The input is a unit step: $x(t) = U(t)$, thus $X(s) = 1/s$:

$$Y(s) = \frac{1}{s[s^2 + s + 1]} : \text{By LT tables: } y(t) = \{1 - 1.1547 e^{-0.5t} \sin[0.8660t + \phi]\}, \phi = \tan^{-1} \frac{\sqrt{1-\xi^2}}{\xi} = 60^\circ$$

C) The input is a unit impulse, so $X(s) = 1$. From tables:

$$y(t) = 1.1547 e^{-0.5t} \sin[0.866 t]$$

2.6 A hyperbolic capacitor discharge waveform results when a capacitor charged to V_o is allowed to discharge through a nonlinear (square law) conductance beginning at time $t = 0$. Kirchoff's current law for this simple circuit is simply: $C \dot{V}_c + \beta V_c^2 = 0$. This ODE can be linearized and solved as Bernoulli's Equation. Since the hyperbolic waveform for $V_c \rightarrow \infty$ at $t = 0$, we delay the start of $V_c(t)$ by τ_o seconds. This yields a hyperbolic waveform section given by $V_c(t) = (C/\beta)/(t + \tau_o)$, for $\tau_o \leq t \leq \infty$. $\tau_o = C/(\beta V_o)$. Thus $V_c(0) = V_o$.

This simple nonlinear circuit is the core of an analog instantaneous pulse frequency demodulator (IPFD) invented by the author; cf. Northrop, R.B. & H.M. Horowitz. 1966. An instantaneous pulse frequency demodulator for neurophysiological applications. *Proc. Symp. Biomed. Engrg. I*, Milwaukee, Wisc. I Biomedical Instrumentation, Paper 1-1, pp 5-8.

2.7 To create a logarithmic hyperbolic capacitor discharge waveform used for generating a log(IPFD), a nonlinear conductance of the form, $i_{nl} = [C k \log_{10} e] 10^{(V_c/k)}$ is used. $e = 2.71828$, k is a constant, and V_c is the capacitor voltage at time t .

$$\begin{array}{lll} \text{2.8 A) } \det \begin{bmatrix} 2 & 3 \\ -1 & 4 \end{bmatrix} = 8 + 3 = 11 & \text{B) } \det \begin{bmatrix} 1 & 0 & 0 \\ 2 & 3 & 5 \\ 4 & 1 & 3 \end{bmatrix} = 1[9 - 5] = 4 & \text{C) } \det \begin{bmatrix} 1 & 0 & 6 \\ 3 & 4 & 15 \\ 5 & 6 & 21 \end{bmatrix} = 1[48 - 90] + 6[18 - 20] = \\ -54. & & \end{array}$$

2.11 Solve the simultaneous equations using Cramer's Rule:

$$\text{A) } 3x_1 - 5x_2 = 0$$

$$x_1 + x_2 = 2 \quad \Delta = \begin{bmatrix} 3 & -5 \\ 1 & 1 \end{bmatrix} = 3 + 5 = 8 \quad x_1 = \begin{bmatrix} 0 & -5 \\ 2 & 1 \end{bmatrix} / \Delta = 10/8, \quad x_2 = \begin{bmatrix} 3 & 0 \\ 1 & 2 \end{bmatrix} / \Delta = 6/8$$

B) $2x_1 + x_2 + 5x_3 + x_4 = 5$
 $x_1 + x_2 - 3x_3 - 4x_4 = -1$
 $3x_1 + 6x_2 - 2x_3 + x_4 = 8$
 $2x_1 + 2x_2 - 2x_3 - 3x_4 = 2$

$$\Delta = \begin{bmatrix} 2 & 1 & 5 & 1 \\ 1 & 1 & -3 & -4 \\ 3 & 6 & -2 & 1 \\ 2 & 2 & 2 & -3 \end{bmatrix} = \dots$$

2.12 $\ddot{y} + 5\dot{y} + 2y = r(t) \rightarrow \dot{x}_1 = 0x_1 + x_2$
 $\dot{x}_2 = -2x_1 - 5x_2 + r(t)$

$$\mathbf{A} = \begin{bmatrix} 0 & 1 \\ -2 & -5 \end{bmatrix} \quad \mathbf{B} = \begin{bmatrix} 0 \\ 1 \end{bmatrix}, \quad \dot{\mathbf{x}} = \mathbf{A}\mathbf{x} + \mathbf{B}r$$

2.13 $2\ddot{y} + 3\dot{y} + y = \dot{r} + 2r \rightarrow \ddot{y} + 1.5\dot{y} + 0.5y = 0.5\dot{r} + r$
 $a_1 \quad a_2 \quad b_1 \quad b_2 \quad b_0 = 0$

The state equations are: $\dot{x}_1 = 0x_1 + x_2 + (0.5)r$
 $\dot{x}_2 = -0.5x_1 - 1.5x_2 + [1 - 1.5(0.5)]r$ Hence $\mathbf{A} = \begin{bmatrix} 0 & 1 \\ -0.5 & -1.5 \end{bmatrix}$ & $\mathbf{B} = \begin{bmatrix} 0.5 \\ -0.25 \end{bmatrix}$

2.14 $\ddot{y} + 3\dot{y} + 2y = 3\ddot{r} + 5\dot{r} + r$ Where: $y = x_1, \dot{x}_1 = x_2$
 $a_1 \quad a_2 \quad b_0 \quad b_1 \quad b_2$

↓

$\dot{x}_1 = x_2 + (5 - 3 \times 3)r$ Hence $\mathbf{A} = \begin{bmatrix} 0 & 1 \\ -2 & -3 \end{bmatrix}$ & $\mathbf{B} = \begin{bmatrix} -4 \\ +7 \end{bmatrix}$
 $\dot{x}_2 = -2x_1 - 3x_2 + [(1 - 2 \times 3) - 3(5 - 3 \times 3)]r$

2.15 A) $H(s) = \frac{s-8}{s^2+3s+2} = \frac{s-8}{(s+1)(s+2)}$ Real zero at $s = +8$, two real poles on the LH s-plane at $s = -1$ & $s = -2$. System is stable.

B) $\frac{s+1}{s^2+3s+3}$ Real zero at $s = -1$. Two complex-conjugate poles in the left-hand s-plane at $s_1 = -3/2 - 1/2 j\sqrt{3}$ and $s_2 = -3/2 + 1/2 j\sqrt{3}$. System is stable.

C) $\frac{s+1}{s^2+3s-3}$ Real zero at $s = -1$. Two real poles; one at $s_1 = -3.7913$, one at $s_2 = +0.7913$ in the RH s-plane. System is unstable.

D) $\frac{s+1}{s^2-3s-3}$ Real zero at $s = -1$. Two real poles; one at $s_1 = +3.7913$ in the RH s-plane, one at $s_2 = -0.7913$. System is unstable.

E) $\frac{s-1}{s^2+3s-4}$ Real zero at $s = +1$. Real poles at $s = -4$ and $s = +1$, System is unstable.

2.16 The SISO linear feedback system's loop gain is: $A_L(s) = \frac{-K(s+8)}{(s-1)(s+6)}$

A) Considering the FB system's root locus diagram, it is stable for two poles in the LH s-plane this is when the RH plane pole locus branch crosses the origin From **Eq. B.5** in the text, the gain must be greater than:

$$K_c > \frac{6 \times 1}{8} = 0.75$$

B) No, one CL system pole is always in the RH s-plane.

2.17 Using Mason's rule:

$$X/Y = \frac{a b c}{1 - [-d -e -bf] + [-d \times -e]} = \frac{a b c}{1 + d + e + bf + de}$$

2.18 The 2I2O LS is described by the ODEs:

$$\begin{aligned} \dot{x}_1 &= -a_{11} x_1 + a_{12} x_2 + b_1 u_1 \\ \dot{x}_2 &= a_{21} x_1 - a_{22} x_2 + b_2 u_2 \end{aligned}$$

A) The SFG is on **Page 6B**.

B) Find X_1/U_1 using Mason's rule:

$$X_1/U_1 = \frac{(b_1/s)[1 - (-a_{22}/s)]}{1 - [-a_{11}/s - a_{22}/s + a_{21}a_{12}/s^2] + [-a_{11}/s \times -a_{22}/s]} = \frac{b_1(s + a_{22})}{s^2 + s[a_{11} + a_{22}] + a_{11}a_{22} - a_{21}a_{12}}$$

C) $X_2/U_2 = \frac{(b_2/s)[1 - (-a_{11}/s)]}{1 - [-a_{11}/s - a_{22}/s + a_{21}a_{12}/s^2] + [-a_{11}/s \times -a_{22}/s]} = \frac{b_2(s + a_{11})}{s^2 + s[a_{11} + a_{22}] + a_{11}a_{22} - a_{21}a_{12}}$

D) $X_1/U_2 = \frac{(b_2/s)(a_{12}/s)}{1 - [-a_{11}/s - a_{22}/s + a_{21}a_{12}/s^2] + [-a_{11}/s \times -a_{22}/s]} = \frac{b_2a_{12}}{s^2 + s[a_{11} + a_{22}] + a_{11}a_{22} - a_{21}a_{12}}$

E) $X_2/U_1 = \frac{(b_1/s)(a_{21}/s)}{1 - [-a_{11}/s - a_{22}/s + a_{21}a_{12}/s^2] + [-a_{11}/s \times -a_{22}/s]} = \frac{b_1a_{21}}{s^2 + s[a_{11} + a_{22}] + a_{11}a_{22} - a_{21}a_{12}}$

2.19 In SS: $\begin{aligned} \dot{x}_1 = 0 &= -a_{11} x_1 + a_{12} x_2 + b_1 U_1 & b_1 U_1 &= a_{11} x_1 - a_{12} x_2 \\ \dot{x}_2 = 0 &= a_{21} x_1 - a_{22} x_2 + b_2 U_2 & b_2 U_2 &= -a_{21} x_1 + a_{22} x_2 \end{aligned} \rightarrow$

Solve using Cramer's rule:

$$\Delta = \begin{vmatrix} a_{11} & -a_{12} \\ -a_{21} & a_{22} \end{vmatrix} = a_{11} a_{22} - a_{21} a_{12}$$

$$X_{1SS} = \frac{\begin{vmatrix} b_1 U_1 & -a_{12} \\ b_2 U_2 & a_{22} \end{vmatrix}}{\Delta} = \frac{b_1 a_{22} U_1 + b_2 a_{12} U_2}{a_{11} a_{22} - a_{21} a_{12}}$$

$$X_{2SS} = \frac{\begin{vmatrix} a_{11} & b_1 U_1 \\ -a_{12} & b_2 U_2 \end{vmatrix}}{\Delta} = \frac{a_{11} b_2 U_2 + a_{12} b_1 U_1}{a_{11} a_{22} - a_{21} a_{12}}$$

2.20 A) From the SFG of **Fig. P2.20**, show $X_2(s)/U_1(s) \rightarrow 0$ for an ideally-decoupled system. There are no cofactors. Note that the bottom dashed feedback path has gain $-a_{21}^*$, not $-a_{22}^*$.

$$X_2/U_1 = \frac{c_1 b_1^{-1} b_1 (1/s) a_{21} (1/s) + c_1 b_1^{-1} b_1 (1/s) (-a_{21}^*) b_2^{-1} b_2 (1/s)}{1 - [-a_{11}/s - a_{22}/s + a_{12} a_{21}/s^2 - a_{12}^* b_1^{-1} b_1 (1/s^2) a_{21} - (P_1 - a_{11}^*) b_1^{-1} b_1 (1/s) - (P_2 - a_{22}^*) b_2^{-1} b_2 (1/s) - a_{22}^* b_2^{-1} b_2 (1/s^2) a_{12}] + \{(-a_{11}/s)(-a_{22}/s) + [-(P_1 - a_{11}^*) b_1^{-1} b_1 (1/s) \times -(P_2 - a_{22}^*) b_2^{-1} b_2 (1/s)] + (-a_{12}^* b_1^{-1} b_1 (1/s^2) a_{21})(-a_{21}^* b_2^{-1} b_2 (1/s^2) a_{12})\}}$$

Reducing the Denominator, D(s): We remove asterisks for ideal decoupling:

$$D(s) = 1 - [-a_{11}/s - a_{22}/s + a_{12} a_{21}/s^2 - a_{12} (1/s^2) a_{21} - (P_1 - a_{11})(1/s) - (P_2 - a_{22})(1/s) - a_{22} (1/s^2) a_{12}] + \{+ a_{11} a_{22}/s^2 + (P_1 - a_{11})(P_2 - a_{22})(1/s^2) + a_{12}^2 a_{21}^2 (1/s^4)\}$$

Reducing the numerator, N(s):

$$N(s) = c_1 a_{21}/s^2 - c_1 a_{21}/s^2 = 0, \text{ Thus } X_2/U_1 = 0, x_2 \text{ is decoupled from input 1.}$$

2.21 A) See **Page 7B** for NLSFG:

B) See **Page 7B** for Decoupled system NLSFG.

C) ODEs for the perfectly-tuned, decoupled system, where: $K_m^* = K_m$, $V_m^* = V_m$, $K_{01}^* = K_{01}$, $K_{12}^* = K_{12}$,

$b_1^* = b_1$, & $b_2^* = b_2$. Thus we have:

$$u_1 = b_1^{-1} [-P_1 x_1 + a_1 v_1 + K_{01} x_1^2 - K_{12} x_2 + V_m x_1/(K_m + x_1)]$$

$$u_2 = b_2^{-1} [-P_2 x_2 + a_2 v_2 + K_{12} x_2 - K_{02} - V_m x_1/(K_m + x_1)]$$

Thus:

$$\begin{aligned} \bullet \quad x_1 &= a_1 v_1 - P_1 x_1 + K_{01} x_1^2 + V_m x_1/(K_m + x_1) - K_{12} x_2 - V_m x_1/(K_m + x_1) - K_{01} x_1^2 + K_{12} x_2 = a_1 v_1 - P_1 x_1 \\ \bullet \quad x_2 &= a_2 v_2 - K_{02} + K_{12} x_2 - V_m x_1/(K_m + x_1) - P_2 x_2 - K_{12} x_2 + V_m x_1/(K_m + x_1) + K_{02} = a_2 v_2 - P_2 x_2 \end{aligned}$$

D) Decoupling controllers for pharmacokinetic drug administration systems are not too effective, because the drug concentrations are non-negative, and 100% effective operation of this kind of controller requires that certain states go negative.